



# A core-shell 2D-MoS<sub>2</sub>@MOF heterostructure for rapid therapy of bacteria-infected wounds by enhanced photocatalysis

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## ABSTRACT

As the increasing antibiotics resistance of bacteria, pathogenic bacterial infections aggravate the skin wounds and prevent it from healing and even induce serious complications. Here, we constructed a core-shell interface electric field at the interface between Prussian blue (PB) metal organic framework (MOF) and two-dimensional MoS<sub>2</sub> nanosheets by *in-situ* growth of MoS<sub>2</sub> on the surface of MOF (MoS<sub>2</sub>@PBMOF), which drove the transfer of photo-excited electrons and promoted the separation of photoinduced electron-hole pairs. Additionally, the lower O<sub>2</sub> adsorption energy of MoS<sub>2</sub>@PBMOF endowed the heterostructure with much stronger O<sub>2</sub> adsorption ability than MoS<sub>2</sub> alone, which provided more oxygen species to capture the photogenerated electrons and holes and thus produced more radical oxygen species (ROS). Meanwhile, the excellent photothermal property of the composite could regulate the release of iron ions from MoS<sub>2</sub>@PBMOF under light irradiation by hyperpyrexia. Hence, under 660 nm visible illumination for 20 min, the MoS<sub>2</sub>@PBMOF killed 99.73 % *S. aureus* and 99.58 % *E. coli*, which attributed to the synergy of local hyperthermia, abundant ROS, and released iron ions through bacterial membrane damage, protein leakage, and the oxidation of glutathione. Importantly, this composite could promote the healing of damaged tissues with good biosafety by promoting the production of hemoglobin. This work provides new insight into the practical application of promising strategy for environmental disinfection and treating bacterial wound infections without using antibiotics.

## 1. Introduction

Pathogenic microbial infections including bacteria and virus induced infectious diseases have been threatening the people's health and even life all over the world. For example, the global coronavirus disease 2019 (COVID-19) pandemics has infected more than 450 million people and killed more than 6 million people [1,2]. According to the clinical reports on COVID-19, many patients died from secondary bacterial infections, especially drug-resistant bacteria infections, rather than from the virus itself [3]. It is difficult to treat bacterial infections effectively until the discovery of penicillin by Alexander Fleming in 1928. Since then, antibiotics were extensively used to treat bacterial infections due to their

broad-spectrum antibacterial effects [4,5]. Unfortunately, owing to the overuse of antibiotics, a large number of antibiotic-resistant bacteria and even super-bacteria occur [6], conventional drugs have not achieved the desired bactericidal effects [7]. It is urgent to develop antibiotics-free strategies to combat pathogenic bacteria, especially multi-drug resistant (MDR) bacteria.

Some inorganic or organic antibacterial agents are commonly used as effective disinfectants such as silver-based antibacterial agents [8], metal oxides (CuO, ZnO, etc.) [9,10], chitosan [11], and antimicrobial peptides [12], which kill bacteria by releasing metallic ions or disrupting membrane integrity to damage the bacterial membrane. Their shortcomings are long sterilization time required for sufficient

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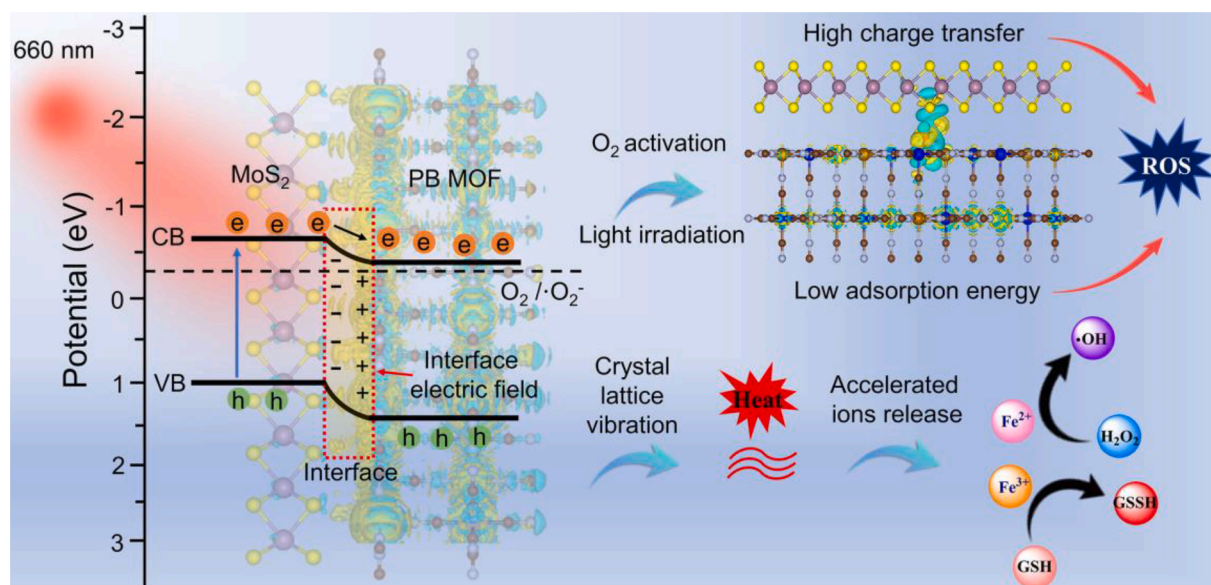
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**Scheme 1.** The schematic illustration of photocatalytic and photothermal effect of MoS<sub>2</sub>@PB for effective bacteria-killing under 660 nm irradiation.

bactericidal efficacy and the long-term cytotoxicity and tissue toxicity induced by these antibacterial agents. For instance, on the one hand, the released metals ions such as Ag<sup>+</sup> and Cu<sup>2+</sup> can accumulate in the main organs and induce lesion [13,14]. On the other hand, some toxic antibacterial ingredients may cause soil and water pollutions during environmental disinfection [15]. Most importantly, the recent studies have shown that bacteria even develop resistance to silver nanoparticles after prolonged contact by genetic variation [16]. In view of these factors, the development of safe, rapid, controllable, and highly effective therapeutic strategies is of great significance and has been attracting more and more attention from scientists and clinicians.

Compared with traditional endogenous antibacterial methods by antibacterial agents themselves, exogenous antibacterial strategies including microwave assisted bactericidal methods [17], ultrasound excited bacteria-killing [18], and light triggered disinfection [19,20], have attracted more and more attention due to the rapid bacteria-killing without inducing bacterial resistance within a short time. Among them, photo-triggered bacteria-killing is portable and low-cost for treating bacterial infected open wounds [21], which generally kills bacteria by photo-triggered hyperthermia locally or photo-produced radical oxygen species (ROS) or the synergistic action of both of them. The deficiency is that highly effective bacteria-killing requires a large amount of ROS or higher temperature of over 60 °C or more locally [22]. However, long time treatment at higher temperatures will destroy healthy tissue and cells [23]. In addition, the yields of ROS produced by photosensitizers are often low because of the following factors. On the one hand, ROS have very short half-life of singlet oxygen (<40 ns) [24], superoxide radicals (1 μs) [25], and hydroxyl radicals (1 ns) [25]. On the other hand, sufficient adsorbed oxygen species and photo-excited electrons and holes are required on the surface of photosensitizers for ROS production. However, most photosensitizers have higher oxygen adsorption energy, which induces low adsorption rate of oxygen species. Furthermore, photo-generated electrons and holes can be recombined easily, which suppressed the photocatalytic performance of photosensitizers. It has been reported that moderate temperature below 55 °C can weaken the bacterial tolerance to ROS by increasing the penetrability of bacterial membrane [26], thus achieving better antibacterial efficiency by the synergy of appropriate quantity of ROS and moderate temperature while ensuring sufficient biosafety [24]. Consequently, there is an urgent need to develop artificial photoresponsive biomedical materials with good photothermal and photocatalytic effects.

Together with its excellent biocompatibility, its two-dimensional

(2D) ultrathin atomic layer structure and high specific surface area endow 2D MoS<sub>2</sub> with excellent photo-electrical performances and promising applications in various field, such as optics [27], catalysis [28], electronics [29], and biomedical fields [30]. Although this material can generate ROS through photocatalysis under 660 nm laser irradiation [31,19], the yield of ROS is very low due to its fast electron-hole recombination and poor oxygen species adsorption ability. Therefore, it is necessary to find other suitable functional materials to combine with MoS<sub>2</sub> to improve the photocatalytic performance by suppressing the recombination of photoexcited electron-hole pairs while reducing its oxygen adsorption energy.

Besides possessing the general priority of metal-organic frameworks (MOFs), such as chemical stability, high specific surface area, high porosity, and effective adsorption of oxygen species [32,33], as a kind of MOF, the Prussian blue (PB) has been clinically approved by the US Food and Drug Administration (FDA). Furthermore, this kind of material has low production cost, low biotoxicity, good photothermal performance, excellent biodegradability, and ease of functionalization [34]. Another priority of this material is that the released Fe<sup>2+</sup> and Fe<sup>3+</sup> ions from PB can react with hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>) and Glutathione (GSH) in the inside of bacteria to generate ·OH and consume GSH [35], thereby accelerating the death of bacteria. Additionally, Fe is an important biological element for physiological activities.

In view of the above mentioned, we propose a hypothesis if a composite composed of 2D MoS<sub>2</sub> and PB MOF can be constructed, which has a lower oxygen species adsorption energy, higher separation efficiency of photoinduced electron-hole pairs, thus producing a large amount of ROS and hyperthermia under visible light irradiation. Consequently, this composite can be used for killing bacteria highly effectively through the synergistic action of locally moderate temperature, large amount of ROS and released ferric ions. In this study, a core-shell heterostructure was constructed using PB MOF as a core and 2D MoS<sub>2</sub> nanosheet as a shell (MoS<sub>2</sub>@PB). As illustrated in Scheme 1, the introduction of PB in the composite structure successfully enhanced the light absorption capacity of MoS<sub>2</sub> under 660 nm illumination, which further improved the photothermal performance of MoS<sub>2</sub>. Meanwhile, formation of MoS<sub>2</sub>@PB heterointerface between the two phases increased the separation efficiency of photoinduced carriers and improved the energy evolution pathways and electrons transfer at the interface, thereby significantly enhancing the photocatalytic activity of MoS<sub>2</sub>, consequently generating more ROS [36,37]. Moreover, the local hyperthermia caused by the photothermal effect will accelerate the release and penetration of iron

ions into the bacteria, promoting Fenton reaction [35] and oxidation of GSH in bacteria. The advantage of this antibacterial agent is that under 660 nm light irradiation, it can quickly and effectively eradicate bacteria within 20 min without the participation of common and toxic antibacterial heavy metal ions (such as  $\text{Zn}^{2+}$ ,  $\text{Cu}^{2+}$ ,  $\text{Ag}^+$ ) and their metal oxides.

## 2. Experimental section

### 2.1. Synthesis of PB nanocubes

The PB nanocubes were prepared through a hydrothermal method. Typically, 748.1 mg  $\text{K}_3[\text{Fe}(\text{CN})_6]$  and 9.91 g PVP were dispersed in 132 mL of HCl (0.01 M) under magnetic stirring for 30 min in a 200 mL reactor. Next, the reactor was placed in a constant temperature oven and heated at 80 °C for 22 h. The synthesized materials were centrifuged (10000 rpm, 15 min) and rinsed by using water and absolute ethanol for 3 times. Finally, the prepared PB nanocubes were collected after vacuum drying at 60 °C for 6 h.

### 2.2. Preparation of $\text{MoS}_2$ @PB

83.1 mg PB and 0.814 g Pluronic F127 were added into 72 mL deionized water under ultrasonic. Then 0.835 g molybdate ( $\text{Na}_2\text{MoO}_4$ ) and 1.398 g of thiocarbamide ( $\text{CN}_2\text{H}_4\text{S}$ ) were added into the mixture. The mixed solution was stirred magnetically at room temperature for 30 min, whereafter transferred to a 100 mL autoclave and heated at 190 °C for 9 h. The solution after reaction was separated via centrifugation at 11 000 rpm for 10 min. The product was rinsed three times using deionized water and absolute ethanol. The obtained samples then were dried at 60 °C under vacuum for 6 h. As a comparison, the  $\text{MoS}_2$  was synthesized the same way as the above method apart from the addition of PB.

### 2.3. Characterization of materials

The microstructure and morphologies were analyzed through field emission scanning electron microscopy (FE-SEM, ZEISS sigma 500, Germany) and transmission electron microscopy (TEM, Japan, JEM-2100F). The XRD spectra were tested by means of X-ray diffraction (D8 ADVANCE, Bruker, Germany) over a diffraction angle ( $2\theta$ ) range of 5° to 80° in 0.01° steps. The nitrogen adsorption and desorption behaviors were obtained by Brunauer-Emmett-Teller (BET, ASAP 2460). UV-vis spectra were measured by an ultraviolet-visible absorption spectrometer (UV-2600, Shimadzu, Japan). XPS spectra were detected by the (Thermo Scientific 250Xi, USA) instrument. Ion release from the material was performed by using the (ICP-AES, Optimal 8000, Perkin Elmer, USA) instrument. PL spectra tests were conducted by a fluorescence spectrometer (LS-55, PerkinElmer). The zeta potential and hydrodynamic diameter were collected on a Dynamic light scattering (DLS) analysis (Malvern, UK).

### 2.4. Photothermal performance measurements of materials

The temperature changes of 400  $\mu\text{g/mL}$  of materials (PBS, PB,  $\text{MoS}_2$  and  $\text{MoS}_2$ @PB) were monitored by a thermal imager (FLIR-E50, Estonia) every-one minute under 660 nm visible light irradiation (0.4  $\text{W/cm}^2$ , 20 min) and images were captured. Temperature changes of  $\text{MoS}_2$ @PB were monitored using a thermal imager during three cycles of 20-minute heating and 20-minute cooling. The photothermal conversion efficiency ( $\eta$ ) of  $\text{MoS}_2$ @PB was calculated in accordance with the following equation [23]:

$$\eta = [hS \times (T_{\max} - T_0) - Q]/[I \times (1 - 10^{-A})]$$

In the formula,  $h$ ,  $S$ ,  $T_{\max}$ ,  $T_0$ ,  $Q$ ,  $I$  and  $A$  denote the heating transfer coefficient, surface area of the heated area, maximum temperature, ambient temperature, heat absorption energy of orifice plate, power of

660 nm laser and absorbance of  $\text{MoS}_2$ @PB at 660 nm, respectively.

During the cooling process, the time constant ( $\tau_s$ ) are calculated according to the following equation:

$$t = -\tau_s \times \ln \theta = \ln(T - T_0)/(T_{\max} - T_0)$$

At this time, assuming that the temperature of the system is very stable, the heat input is equal to the heat output, and the following equation is used:

$$hS = m_s \times C_s / \tau_s$$

In the formula,  $m_s$  and  $C_s$  are the mass and specific heat capacity of water, respectively.

### 2.5. Photoelectrochemical measurements of materials

The photoelectrochemical properties of the samples were determined by a three-electrode electrochemical workstation (CHI660E, China), in which the platinum electrode was used as counter electrode, the Ag/AgCl electrode was used as reference electrode, and the sample groups were employed as the working electrode. The photocurrent response and EIS measurements of the samples were carried out with 660 nm visible light as the light source (power 0.4  $\text{W/cm}^2$ ) and 0.5 M sodium sulfate aqueous solution as the electrolyte. The working electrode was prepared as follows: 4 mg sample powder was dispersed in 1 mL absolute ethanol, and then 150  $\mu\text{L}$  of naphthol solution was added to form a uniform dispersion under ultrasonication. Finally, 50  $\mu\text{L}$  of the above dispersed droplets were placed on the treated titanium sheet with a diameter of 6 mm and dried for 6 h in a 50 °C oven to acquire the required working electrode.

### 2.6. Photodynamic measurements of materials

In order to study  $^1\text{O}_2$  produced by the samples under 660 nm irradiation, 1,3-diphenyliso-benzofuran (DPBF) was used as an indicator. By calculating the absorption drop at 425 nm [38], the  $^1\text{O}_2$  produced during photocatalysis was determined. Nitro blue tetrazolium (NBT) dimethyl sulfoxide (DMSO) solution ( $2.5 \times 10^{-6}$  mol/L) can react with superoxide radical ( $\cdot\text{O}_2^-$ ) to form monoformazan (MF) [39,40]. Therefore, the production of  $\cdot\text{O}_2^-$  after irradiation can be examined by comparing the absorbance of MF. Hydroxyl radical ( $\cdot\text{OH}$ ) was determined by terephthalic acid (TA) NaOH solution (4 mM) because their reaction product of 2-hydroxyl terephthalic acid (TAOH) had characteristic fluorescence excited by 312 nm at 450 nm [39,40]. The  $\cdot\text{O}_2^-$  and  $\cdot\text{OH}$  of samples were further detected by electron spin resonance (ESR, Bruker EMXplus, Germany) spectroscopy with 5, 5-dimethyl-1-pyrrolin-N-oxide (DMPO) as a spin trap under 660 nm red light [41,42].

### 2.7. Theoretical calculations

We carried out first-principle calculations in the DFT framework using the Vienna AB Initio simulation package (VASP). The exchange correlation energy was described by the Perdew-Burke-Ernzerhof (PBE) form of the generalized Gradient Approximation (GGA) exchange correlation energy functional, in combination with the DFT-D3 correction. The structure optimization of  $\text{MoS}_2$  and PB has been performed by changing the positions of all atoms and fixing the lattice parameters until the energy difference of the continuous atomic configuration was  $<10^{-4}$  eV. The force per atom in the relaxed structure was  $<0.015$  eV/Å. The cutoff energy of the plane wave basis set was set to 400 eV. The k-point spacing on the Brillouin zone (BZ) was set to be  $<0.03$  Å $^{-1}$ . The isolated  $\text{O}_2$  molecule was put in  $10$  Å  $\times$   $10$  Å  $\times$   $10$  Å lattices to perform the structure optimizations.

To calculate the adsorption energies of  $\text{O}_2$  molecules on PB,  $\text{MoS}_2$  surfaces and  $\text{MoS}_2$ @PB heterojunction, we first constructed the corresponding surfaces. In order to obtain the most stable structures, their structure optimizations were performed by fixing bottom 2 layers and

setting the thickness of 15 Å vacuum. Adsorption energy calculation formula is as follows:

$$\Delta E = E_{\text{system}} - E_{\text{slab}} - E_{\text{adsorbate}}$$

In the formula,  $E_{\text{system}}$ ,  $E_{\text{slab}}$  and  $E_{\text{adsorbate}}$  denote the total energies of the adsorption system, substrate surface and adsorbate, respectively.

## 2.8. In vitro antimicrobial experiments

The antimicrobial ability of materials (PB, MoS<sub>2</sub>, MoS<sub>2</sub>@PB) was investigated using *S. aureus* and *E. coli* through the spread plate experiment. Firstly, all samples and equipment involved in the experiment were irradiated with an ultraviolet lamp for 30 min in advance for disinfection. Then, 20 µL sterile PBS (control group) or 4 mg/mL of the sample solution (PB, MoS<sub>2</sub>, or MoS<sub>2</sub>@PB) were aspirated to a 96-well plate containing 180 µL bacterial suspension ( $1 \times 10^7$  CFU/mL). Each sample group was divided into dark and light group. The samples in the dark group were covered with tin foil and placed for 20 min to eliminate the influence of light, while the samples in the light group were exposed to a 660 nm laser (0.4 W/cm<sup>2</sup>) for 20 min, but the temperature was maintained at about 55 °C.

After that, the *S. aureus* and *E. coli* suspensions in each well were diluted 100-fold, and 20 µL the diluted bacterial liquid was pipetted and spread equably on the agar plate. The agar plates were placed in a incubator at 37 °C for 1 day, and then the number of colony was counted. Finally, the antimicrobial efficacy was calculated in accordance with the following equation (in which D is the Colony Forming Unit): Antimicrobial efficacy (%) = (D in control group – D in experimental group)/D in control group × 100 %.

In the cycles of bacteria-killing tests, cultured bacteria ( $1 \times 10^9$  CFU/mL) were diluted to  $1 \times 10^7$  CFU/mL. Then at the end of each antimicrobial test, 200 µL of the bacterial solution was incubated again in fresh medium and used for the next cycle. To evaluate the influence of hyperthermia or ROS alone on the antibacterial performance of MoS<sub>2</sub>@PB, the experiments were divided into four groups: Control, MoS<sub>2</sub>@PB + Light (19 °C), MoS<sub>2</sub>@PB + Water-bath (55 °C), and MoS<sub>2</sub>@PB + Light (55 °C). Notably, the temperature of the MoS<sub>2</sub>@PB + Water-bath (55 °C) and MoS<sub>2</sub>@PB + Light (55 °C) increased for 7 min and kept at 55 °C for 13 min, while the MoS<sub>2</sub>@PB + Light (19 °C) group maintained a 19 °C warming and cooling balance in an ice-water bath. The antibacterial experiment of materials under visible light irradiation was performed by 300 W xenon light (0.2 W/cm<sup>2</sup>). The method and operational details of the antibacterial experiments are the same as for the 660 nm laser.

## 2.9. Morphology observation of bacteria

After the antibacterial experiment, the bacterial liquid in the 96-well plate was first abandoned, and then rinsed with sterile PBS for 3 times. Next, 200 µL 2.5 % glutaraldehyde diluent was pipetted to each well, followed by fixation for 2 h. Each well was rinsed for 3 times using sterile PBS, 200 µL ethanol with different concentration gradients (30 %, 50 %, 70 %, 90 %, 100 %) were added and dehydrated for 15 min. Finally, after waiting for the samples to dry, the morphologies of the bacteria were observed with a scanning electron microscope and photographed.

## 2.10. Live/dead fluorescent staining of bacteria

To visually observe the live/dead states of bacteria, the live/dead fluorescence experiment of bacteria was performed. The samples were mixed with bacteria solution ( $1 \times 10^7$  CFU/mL) and then irradiated with 660 nm visible light for 20 min. The bacterial suspension without the materials was used for the control group. After the antimicrobial operation was completed, the bacteria after different treatments were stained using SYTO9 and PI (Baclight bacterial viability kit, Invitrogen) for 20 min simultaneously and then rinsed with sterile PBS. The photographs were taken with an inverted fluorescence microscope (Olympus, IFM,

IX73).

## 2.11. Protein leakage in bacteria

Bichinchonic acid (BCA) protein assay was adopted to quantitatively determine protein leakage from bacteria. Briefly, after completion of bactericidal experiment, the 150 µL diluted bacterial liquid was mixed with 150 µL sterile PBS, and centrifuged by 6000 rpm for 6 min. Then 25 µL the supernatant was added to 200 µL BCA reagent, and the relative protein leakage was determined on a microplate reader at OD<sub>562 nm</sub>.

## 2.12. Ellman's assay

GSH depletion was evaluated using the Ellman's assay [43,44]. In brief, the samples were mixed with 150 µL of GSH bicarbonate buffer solution (0.8 mM) in a 48-well plate and then cocultured at room temperature for 10 min to achieve the equilibrium of adsorption and desorption. Afterwards, the samples were irradiated with a 660 nm laser for 20 min. Subsequently, the supernatant was added into 100 µL 5,5'-dithio-bis-(2-nitrobenzoic acid) (DTNB) (10 mM) and 450 µL Tris-HCl (pH = 8.0, 50 mM), and shook for 20 min to adequately react. As negative control and positive control, 100 µL of PBS and 30 % H<sub>2</sub>O<sub>2</sub> were added into 200 µL of GSH solution (0.8 mM), respectively. Finally, the consumption of GSH was calculated through determining the absorbance values at 410 nm on a microplate reader.

## 2.13. Permeability determination of bacterial membrane

The *ortho*-nitrophenyl-β-galactoside (ONPG) assay was conducted to determine the permeability of the membrane (cytoplasmic panniculus) of *S. aureus* on the surface of the samples [45,26]. After the antibacterial process was completed under 660 nm light irradiation or dark conditions, the samples were treated with an ONPG assay kit. The absorbance of supernatant at 420 nm was measured with a microplate reader.

## 2.14. Cytocompatibility evaluation in vitro

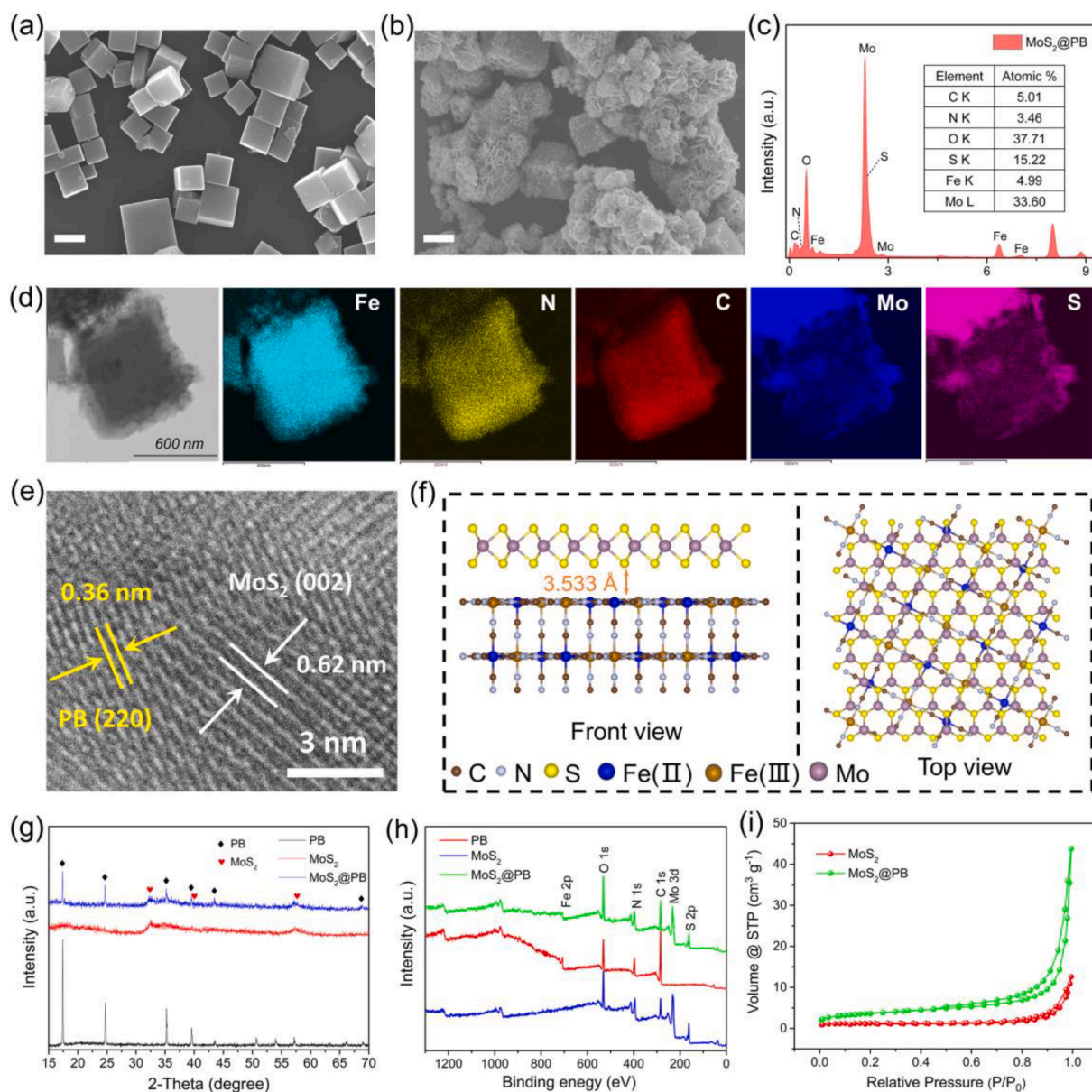
### 2.14.1. Cell culture and MTT assay

NIH-3 T3 fibroblast cells (Tongji Hospital, Wuhan) were selected as a model to assess the cytotoxicity of different materials using a MTT test. The NIH-3 T3 cells were cocultured with Dulbecco's Modified Eagle Medium (DMEM) including 10 % fetal calf serum and 1 % penicillin–streptomycin solution at 37 °C in a 5 % CO<sub>2</sub> incubator. Before the assay, all materials and equipment were sterilized with 75 % alcohol and a UV lamp about 30 min. The diluted cells suspensions ( $1 \times 10^5$  cells/mL) and different materials were added into the 96-well plate and cocultured for 1, 3 and 7 days, respectively. After that, the DMEM medium was displaced by 200 µL of prepared MTT solution (0.5 mg/mL) and therewith further cultivated at 37 °C for 4 h. Next, the MTT solution in the plate was removed completely, and 200 µL DMSO solution was aspirated into each well with continuous shaking for 20 min to fully dissolve the crystals. The OD value at 490 nm and 570 nm were measured using a microplate reader. The cell viability of samples was obtained through comparing the OD values of each group.

### 2.14.2. Cell fluorescence staining

To intuitively observe cell morphology, a cell fluorescence staining assay was performed in this experiment. First, the NIH-3 T3 cells and materials were cocultured for 1 day in a 96-well plate. After removing the supernatant solution, the cells spreading on samples rinsed with sterile PBS for 3 times, and therewith immobilized by 4 % formaldehyde for 15 min. Afterwards, the NIH-3 T3 cells were subsequently stained by FITC (YiSen, Shanghai) for 30 min in darkness and rinsed with PBS several times. After that, DAPI (YeaShen, Shanghai) was used to stain the cells for 30 s and then rinsed again with PBS. Finally, the cell morphology on the surface of the samples were observed by an inverted





**Fig. 1.** FE-SEM of (a) PB MOF and (b) MoS<sub>2</sub>@PB (scale bars = 500 nm). (c) TEM-EDX of MoS<sub>2</sub>@PB. (d) TEM images and corresponding EDX mapping of MoS<sub>2</sub>@PB. (e) HRTEM of MoS<sub>2</sub>@PB. (f) Crystal structure of MoS<sub>2</sub>@PB of different perspectives after structure optimization. (g) XRD of PB, MoS<sub>2</sub> and MoS<sub>2</sub>@PB. (h) The XPS survey spectrum of PB, MoS<sub>2</sub> and MoS<sub>2</sub>@PB. (i) The nitrogen adsorption and desorption of PB and MoS<sub>2</sub>@PB.

fluorescence microscope.

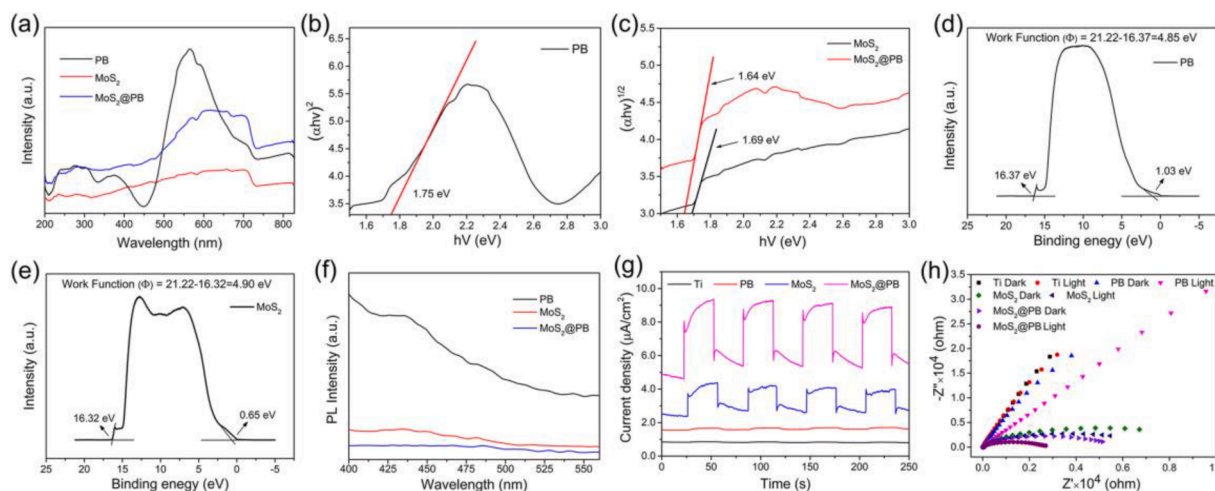
### 2.15. Hemolytic test

Hemolysis tests of the materials were performed with fresh mouse's blood. The fresh blood was centrifuged (3000 rpm/min, 15 min) and then the serum was removed to collect red blood cells. The red blood cells were rinsed with normal saline three times. Subsequently, 500  $\mu$ L of a saline solution of materials (800 ppm) were added in 500  $\mu$ L of a 10 % red blood cell dispersion, respectively. As control, 500  $\mu$ L of deionized water or normal saline and 500  $\mu$ L of 10 % red blood cell dispersion were uniformly mixed in a centrifuge tube as a positive control and a negative control, respectively. The mixture was then incubated at 37  $^{\circ}$ C for 4 h. After centrifugation (3000 rpm/min, 15 min) at 4  $^{\circ}$ C, 100  $\mu$ L of supernatant solution was aspirated into a 96-well plate, and the absorbance at 570 nm was tested with a microplate reader. The material hemolytic rates (RHR%) were calculated as follows:  $RHR (\%) = (A_{\text{sample}} - A_{\text{negative}}) / (A_{\text{positive}} - A_{\text{negative}})$ . A is the absorbance at 570 nm of the

supernatant.

### 2.16. In vivo antimicrobial experiments

All experimental protocols were agreed by Prevention and the Animal Experiment Center of Huazhong Agricultural University and the Hubei Provincial Center for Disease Control. The test procedure was carried out in accordance with the "Guidelines for the Care and Use of Laboratory Animals in China" and "Regulations on Animal Management of the Ministry of Health of the People's Republic of China". Balb/c male mice (6–8 weeks old,  $\sim$ 25 g in body weight) were obtained from the animal test center of Huazhong Agricultural University. The mice were randomly assigned to one of three groups: Control, 3 M and MoS<sub>2</sub>@PB groups. Because of the rapid sterilization, the wound was treated only once, and the wound was treated as follows. Before surgery, 10 % chloral hydrate (30 mg/kg) was injected intraperitoneally into each mouse for anesthesia. The mice were first shaved, then the backs of the mice were then slashed and a biopsy punch was used to create two symmetrical



**Fig. 2.** (a) UV-vis absorption spectra of different groups. (b) Band gap of PB. (c) Band gap of MoS<sub>2</sub> and MoS<sub>2</sub>@PB. UPS spectra of (d) PB, and (e) MoS<sub>2</sub>. (f) PL spectra of PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB by 325 nm excitation wavelength. (g) Photocurrent response under 660 nm laser irradiation. (h) EIS spectra.

circular wounds of 8 mm in diameter on the left and right sides of each mouse's spine. Subsequently, the wounds of each group were infected with *S. aureus* ( $1 \times 10^8$  CFU/mL, 10  $\mu$ L) to build an infection model. For the control and 3 M groups, the wounds were disposed of by a 10  $\mu$ L sterile PBS. Comparatively, in the material group, the wounds were disposed of by using 10  $\mu$ L MoS<sub>2</sub>@PB (0.8 mg/mL). After being irradiated with 660 nm laser for 20 min, the wounds of control and MoS<sub>2</sub>@PB groups were covered using hospital gauze. The treated wounds in the 3 M group were bandaged using standard 3 M wound dressings. Then, the mice were raised singly in cages at standard temperature.

Giemsa staining and H&E staining were used to observe wound healing. After 2, 5, 8, 12, and 14 days, photographs of wounds in mice were taken, respectively. Giemsa staining and H&E staining of tissue from the wounds were performed to observe the number of bacteria, inflammation cells, and wound healing process around the wound. Finally, main organs (heart, liver, spleen, lung, and kidney) were collected on day 14 and H&E staining was photographed to assess the *in vivo* biotoxicity of different samples.

### 2.17. Statistical analysis

All experimental data were expressed as mean  $\pm$  standard deviation (SD) with  $n \geq 3$ . Statistical significance was estimated using an unpaired *t*-test. The *p*-value was analyzed using one-way or two-way analysis of variance (ANOVA) and specified in the figure legends.

## 3. Results and discussion

### 3.1. Characterization of MoS<sub>2</sub>, PB and MoS<sub>2</sub>@PB

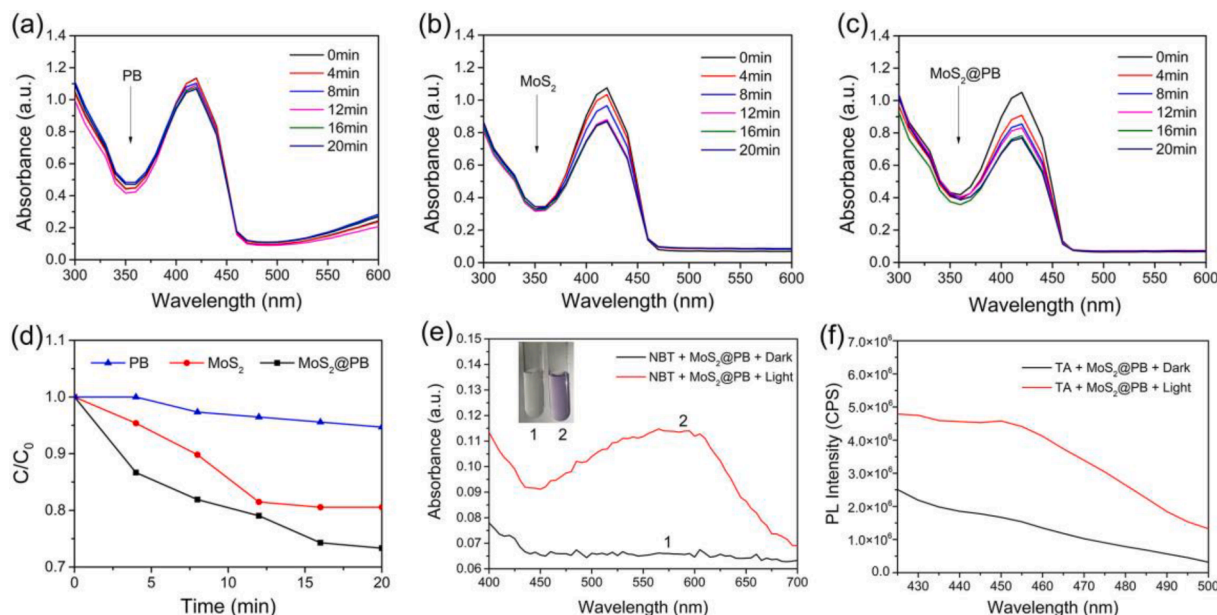
The morphologies of prepared materials (MoS<sub>2</sub>, PB, MoS<sub>2</sub>@PB) were exhibited in Fig. 1a, 1b, and S1, respectively. Field-emission scanning electron microscopy clearly exhibited that PB MOF was a regular nanocube and MoS<sub>2</sub> was a nanosphere interwoven with two-dimensional nanosheets. What was more, it could be clearly observed from the morphologies of synthesized MoS<sub>2</sub>@PB composite that regular two-dimensional MoS<sub>2</sub> nanosheets have grown *in situ* on the surface of PB. The scale bar measurement showed that the average size of single PB and MoS<sub>2</sub>@PB was about 300 nm and 650 nm, respectively, which were well in line with the measurement results of the DLS (Fig. S2). DLS exhibited that the average particle sizes of PB and MoS<sub>2</sub>@PB composite in PBS were about 283.0 nm and 692.4 nm, respectively. Meanwhile, the TEM image in Fig. 1d and S3 showed that MoS<sub>2</sub>@PB had a typical core-shell heterostructure, with PB as the inner core and MoS<sub>2</sub> nanosheets

as the outer shell.

Energy-dispersive X-ray spectroscopy (EDS) (Fig. 1c) demonstrated that MoS<sub>2</sub>@PB contained all elements of PB and MoS<sub>2</sub> (Figs. S4 and S5), indicating coexistence of the two materials. According to the EDX mapping (Fig. 1d), Fe, N, and C elements were located at the nucleus, while Mo and S were mainly distributed in the outer shell, indicating 2D MoS<sub>2</sub> nanosheets were homogeneously distributed on the surface of PB. Furthermore, the core-shell heterointerface of MoS<sub>2</sub>@PB could be clearly observed in Fig. 1e and S6 through high-resolution transmission electron microscopy (HRTEM), where the lattice fringe spacing of 0.62 nm and 0.27 nm belonged to the typical (0 0 2) and (1 0 0) planes of MoS<sub>2</sub> [32], while the lattice fringe spacing of 0.36 nm and 0.50 nm belonged to the typical (2 2 0) and (2 0 0) planes of PB phase [35]. Fig. 1f showed the atomic structure of the MoS<sub>2</sub>@PB heterojunction. According to the density functional theory (DFT) calculation, a stabilized crystal structure was formed and corresponding interface space between PB and MoS<sub>2</sub> was about 3.533 Å, indicating that they are tightly bound.

As shown in Fig. 1g, XRD spectra showed the diffraction peaks at 32.6°, 39.9°, and 57.3°, corresponding to the (1 0 0), (1 0 3), and (1 1 0) crystal face of MoS<sub>2</sub> [46,28], which were also present in MoS<sub>2</sub>@PB (marked as MoS<sub>2</sub> with red hearts), indicating that the combination with PB did not change the crystallographic structures of MoS<sub>2</sub>. Additionally, the typical crystal face of 17.6° (2 0 0), 24.9° (2 2 0), 35.4° (4 0 0), 39.7° (4 2 0), 43.7° (4 2 2), and 69.2° (6 4 2) of the PB phase also existed in MoS<sub>2</sub>@PB (black diamonds marked as PB) [22], indicating the successful modification of MoS<sub>2</sub> onto PB surfaces. Moreover, in Fig. S7, the zeta potential value of PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB were -20.0, -33.7, and -25.2 mV, respectively, and the potential of MoS<sub>2</sub>@PB was between PB and MoS<sub>2</sub>, indicating that MoS<sub>2</sub> changes its surface charge after growing on the surface of PB MOFs.

X-ray photoelectron spectroscopy (XPS) spectrum (Fig. 1h) showed PB contained four elements C, N, O, and Fe. After MoS<sub>2</sub> nanosheets grew on it, strong signals of Mo and S appeared together with C, N, O, and Fe in spectrum. The Fe 2p high-resolution XPS spectrum of MoS<sub>2</sub>@PB (Fig. S8a) had two main peaks at 708.9 and 721.8 eV, belonging to Fe 2p<sub>1/2</sub> and Fe 2p<sub>3/2</sub> of Fe<sup>3+</sup>, respectively, and satellite peaks at 712.8 and 725.9 eV corresponding to Fe<sup>2+</sup>, indicating that Fe in MoS<sub>2</sub>@PB exhibited a hybrid valence state [22]. The main peaks of C 1s and N 1s were at 284.9 eV and 398.1 eV, respectively, which could prove the existence of C-N([Fe(CN)<sub>6</sub>]<sup>4-</sup>) in the materials (Fig. S8b and S8c). As shown in Fig. S8d, the binding energies of 232.6 eV and 228.9 eV were attributed to Mo 3d<sub>3/2</sub> and Mo 3d<sub>5/2</sub> of Mo<sup>4+</sup> [47,48]. Besides, the S 2p spectra of S 2p<sub>1/2</sub> and S 2p<sub>3/2</sub> identified at 161.7 eV and 163.1 eV (Fig. S8e), respectively, which proved the existence of MoS<sub>2</sub> in the



**Fig. 3.** The  $^1\text{O}_2$  detected by DPBF degradation of (a) PB, (b)  $\text{MoS}_2$ , and (c)  $\text{MoS}_2@\text{PB}$  under 660 nm laser irradiation. (d) Contrast curve between PB,  $\text{MoS}_2$ , and  $\text{MoS}_2@\text{PB}$ . (e)  $\cdot\text{O}_2$  detection of  $\text{MoS}_2@\text{PB}$  using NBT method. (f)  $\cdot\text{OH}$  detection of  $\text{MoS}_2@\text{PB}$  using TA.

$\text{MoS}_2@\text{PB}$  composite [49]. Fig. S8f showed the O 1 s spectrum. This result further confirms the formation of a core-shell heterostructure with the inner core as PB and the outer shell as  $\text{MoS}_2$ .

The nitrogen adsorption/desorption experiment was performed to characterize the BET surface area of the material. On the basis of Fig. 1i, the BET surface area of  $\text{MoS}_2$  increased from  $4.067 \text{ m}^2/\text{g}$  to  $12.862 \text{ m}^2/\text{g}$  after combining with PB MOFs, demonstrating that the introduction of PB improved the BET surface area of  $\text{MoS}_2$ . PB MOF had a specific surface area of  $297.817 \text{ m}^2/\text{g}$  in Fig. S9.

The above characterization studies confirm that  $\text{MoS}_2$  is uniformly dispersed on PB from multiple perspectives, forming a structurally stable  $\text{MoS}_2@\text{PB}$  nanocomposite.

### 3.2. Photoelectrochemical test and band structure

The optical performance of the material was determined on a UV–vis diffuse reflectance spectroscopy, and Fig. 2a compared the UV–visible absorption among samples. The red curve in the figure showed that the absorption of  $\text{MoS}_2$  was primarily in the visible range, but the absorption was weak. The black and blue curves represented PB and  $\text{MoS}_2@\text{PB}$ , respectively. Compared with  $\text{MoS}_2$ , the introduction of PB dramatically improved the absorption of  $\text{MoS}_2@\text{PB}$  in the visible range due to the strong absorption of PB, especially at the range of 500–720 nm. Hence,  $\text{MoS}_2@\text{PB}$  had a larger light absorption capacity than  $\text{MoS}_2$ .

To evaluate the production and transfer of photogenerated charges, the bandgap energy of the samples was calculated as follows. In accordance with the plot of the Kubelka-Munk function versus bandgap energy, the energy gap of PB,  $\text{MoS}_2$ , and  $\text{MoS}_2@\text{PB}$  were counted to be 1.75, 1.69, and 1.63 eV (Fig. 2b and 2c), respectively, suggesting that the calculated bandgap of  $\text{MoS}_2@\text{PB}$  was obviously red-shifted compared to  $\text{MoS}_2$ , which was beneficial to the generation of more photo-excited electrons under 660 nm laser irradiation. Furthermore, the UV photoelectron spectroscopy (UPS) was employed to calculate the band potential of PB and  $\text{MoS}_2$  (Fig. 2d and 2e). According to Han et al [50], the corresponding work functions ( $\Phi$ ) of PB and  $\text{MoS}_2$  were 4.85 and 4.90 eV, respectively, while the difference between the  $\Phi$  and the valence band (VB) were 1.03 and 0.65 eV, respectively. Therefore, the VB and conduction band (CB) of PB versus NHE were 1.38 and  $-0.37 \text{ eV}$ , respectively, and the VB and CB of  $\text{MoS}_2$  versus NHE were 1.05 and  $-0.64 \text{ eV}$ , respectively.

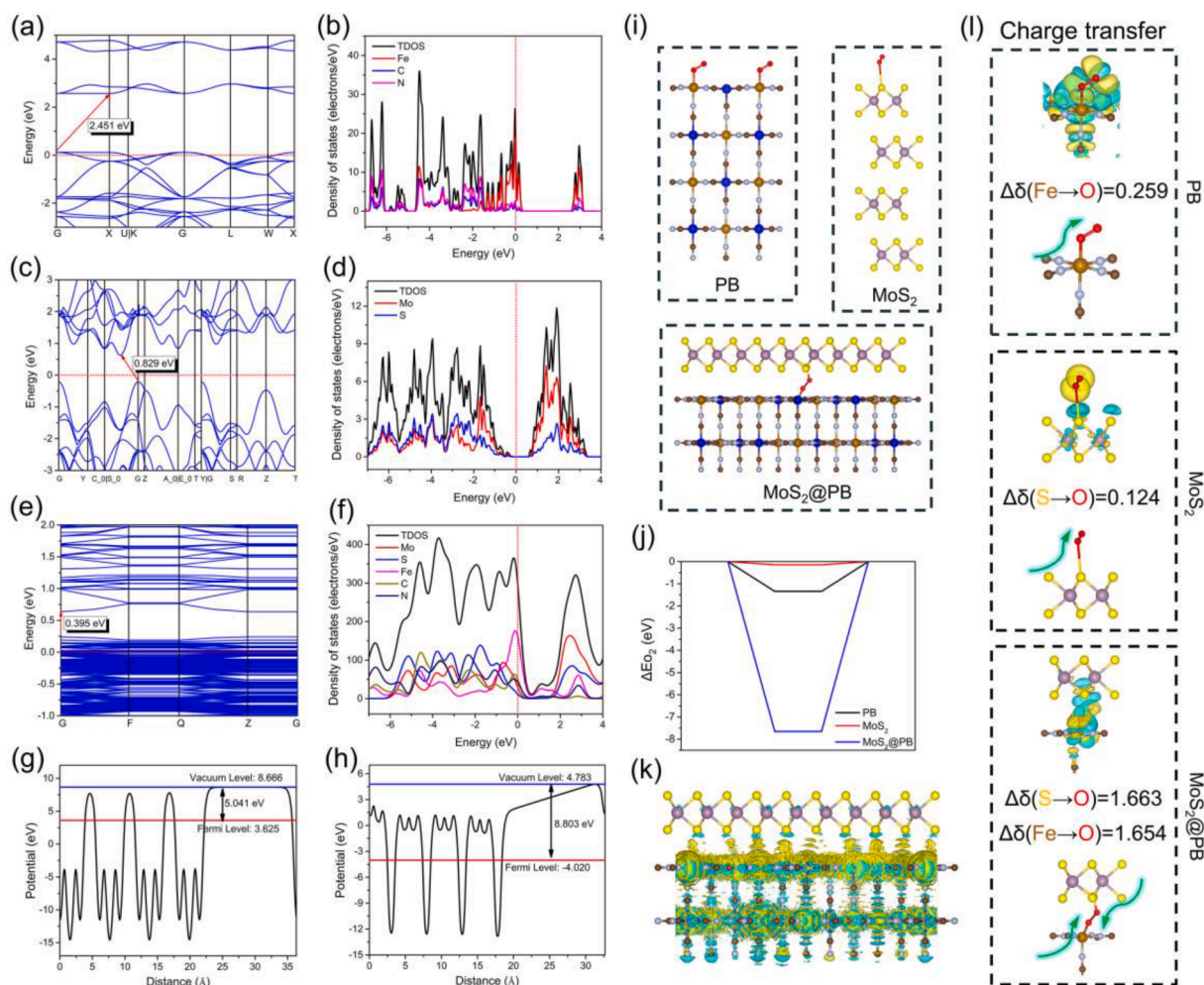
The photoluminescence (PL) of the material is mainly because of the recombination of photogenerated carriers. Fluorescence spectroscopy is usually used to probe the migration and recombination process of photogenerated charges in semiconductors, and the decrease in fluorescence intensity means that the probability of carrier recombination decreases. In general, with the decrease of fluorescence intensity, the recombination probability of photogenerated carriers in this sample decreases, which indicated this sample has better photocatalytic performance [51]. The PL spectra in Fig. 2f exhibited that the fluorescence intensity of  $\text{MoS}_2@\text{PB}$  at about 435 nm was lower than that of PB and  $\text{MoS}_2$ . The weaker fluorescence emission peak suggested the lower electron-hole recombination rate in  $\text{MoS}_2@\text{PB}$ . This result may reflect the rapid transfer of photoinduced electrons from  $\text{MoS}_2$  to PB along the heterointerface, hindering the recombination of photoinduced carriers. Therefore, the electron-hole separation efficiency of  $\text{MoS}_2@\text{PB}$  nanocomposites is improved [52].

Additionally, electrochemical impedance spectroscopy (EIS) and transient photocurrent response were used to verify this conclusion. The photocurrent density was measured to evaluate the charge transfer ability of photocatalyst materials. In Fig. 2g, the photocurrents of PB,  $\text{MoS}_2$ , and  $\text{MoS}_2@\text{PB}$  exhibited good stability and reproducibility in four switching cycles under 660 nm laser irradiation. It was evident that  $\text{MoS}_2@\text{PB}$  had the highest photocurrent density ( $3.51 \mu\text{A}/\text{cm}^2$ ), which was much larger than other photocurrent density of PB and  $\text{MoS}_2$  ( $1.39 \mu\text{A}/\text{cm}^2$ ), suggesting that  $\text{MoS}_2@\text{PB}$  had a faster charge separation efficiency [53]. Thus,  $\text{MoS}_2@\text{PB}$  exhibited the best photocatalyst property. The EIS tests were performed to determine the impedance of photocatalyst materials. Generally, the smaller semicircle arc in the EIS suggests a smaller electrical resistance [54]. As shown in Fig. 2h,  $\text{MoS}_2@\text{PB}$  had the smallest arc compared to PB and  $\text{MoS}_2$ , indicating that  $\text{MoS}_2@\text{PB}$  had the highest charge separation efficiency and smallest charge transfer resistance. Moreover, the impedance of the light groups was smaller than that of the dark groups. These results all confirmed that the photocatalytic activity of  $\text{MoS}_2@\text{PB}$  was significantly enhanced after  $\text{MoS}_2$  combined with PB, which was beneficial to promote the ROS yield.

### 3.3. Photocatalytic and photothermal properties

ROS including  $^1\text{O}_2$ ,  $\cdot\text{O}_2^-$ , and  $\cdot\text{OH}$  is a strong oxidant. It is an active substance generated by the reaction of photogenerated charges with





**Fig. 4.** Electronic band structure and density of states (DOS) of PB (a, b), MoS<sub>2</sub> (c, d) and MoS<sub>2</sub>@PB (e, f). The calculated work function of PB (g) and MoS<sub>2</sub> (h). (i) Crystal structures after oxygen absorption on PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB. (j) Adsorption energy of oxygen on the surfaces of PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB. (k) 3D charge density difference of MoS<sub>2</sub>@PB. (l) Bader charge calculations of adsorbent O<sub>2</sub>.

oxygen or water molecules in the environment [55], which can destroy the oxygen balance inside the bacteria and has a good bacteria-killing ability. The 1,3-diphenylisobenzofuran (DPBF) was utilized to detect the singlet oxygen (<sup>1</sup>O<sub>2</sub>) production of materials by a 660 nm visible illumination. The absorption intensity of DPBF at 420 nm was decreased when specifically reacting with <sup>1</sup>O<sub>2</sub> [38]. As shown in Fig. 3a, the absorption intensity of the PB group basically unchanged with the extension of the irradiation time, suggesting that PB produce no <sup>1</sup>O<sub>2</sub> under irradiation. By contrast, the absorption peak intensity of MoS<sub>2</sub>@PB group and MoS<sub>2</sub> group at 420 nm decreased gradually, and MoS<sub>2</sub>@PB decreased more quickly than MoS<sub>2</sub> (Fig. 3b and 3c), indicating that the introduction of PB greatly improved the photodynamic performance of MoS<sub>2</sub>. In addition, the contrast curve further intuitively showed that MoS<sub>2</sub>@PB exhibited a higher <sup>1</sup>O<sub>2</sub> yields than MoS<sub>2</sub> (Fig. 3d).

To further explore ROS types, nitroblue tetrazolium (NBT) and terphthalic acid (TA) were employed to investigate the ·O<sub>2</sub><sup>-</sup> and ·OH generation of MoS<sub>2</sub>@PB, respectively. As shown in Fig. 3e and 3f, compared with the dark conditions, the absorption peak of monoformazan (MF) from 450 to 700 nm and the fluorescence emission peak of 2-hydroxyl terephthalic acid (TAOH) at 450 nm of MoS<sub>2</sub>@PB showed characteristic absorption peak after illumination respectively, implying the existence of ·O<sub>2</sub><sup>-</sup> and ·OH [39,40]. In addition, the ·O<sub>2</sub><sup>-</sup> and ·OH of samples were further detected using the electron spin resonance (ESR) spectroscopy [41,42], respectively. As shown in Fig. S10, there were obvious signals for ·O<sub>2</sub><sup>-</sup> and ·OH detected under light illumination,

indicating the production of ·O<sub>2</sub><sup>-</sup> and ·OH [41,42].

To study the photocatalytic mechanism of MoS<sub>2</sub>@PB heterostructure, the band structure and density of states of PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB were calculated by the first-principles calculations. The Fermi level was set as 0 eV for reference. Fig. 4a and 4c showed the calculated bandgaps of the PB, MoS<sub>2</sub> were 2.451 and 0.829 eV, respectively. When the monolayer MoS<sub>2</sub> was adsorbed on the surface of PB, the valence band maximum (VBM) of the composite system moved towards the Fermi level obviously, decreasing the band gap to 0.395 eV (Fig. 4e). The calculated energy band showed the same decreasing tendency as the previous experimental results, which may be due to the strong interaction between PB and MoS<sub>2</sub>. Simultaneously, compared with PB and MoS<sub>2</sub> (Fig. 4b and 4d), the corresponding DOS results of MoS<sub>2</sub>@PB heterostructure displayed more hybridization at the Fermi level, suggesting that electron transfer and interfacial reaction occurred between PB and MoS<sub>2</sub> (Fig. 4f).

To probe the process of interface charge transfer in the MoS<sub>2</sub>@PB heterojunction, the calculated work function of the PB and MoS<sub>2</sub> were calculated through DFT calculations [56]. In Fig. 4g and 4h, the work functions of the PB and MoS<sub>2</sub> were 5.041 eV and 8.803 eV, respectively. This suggested that the Fermi energy level corresponding to MoS<sub>2</sub> was lower than PB. As a result, electrons from the PB surface could transport to the MoS<sub>2</sub> surface through the interface when in close contact with MoS<sub>2</sub> in the dark. Therefore, this confirmed that an interfacial electric field can be established because of the redistribution of charges between



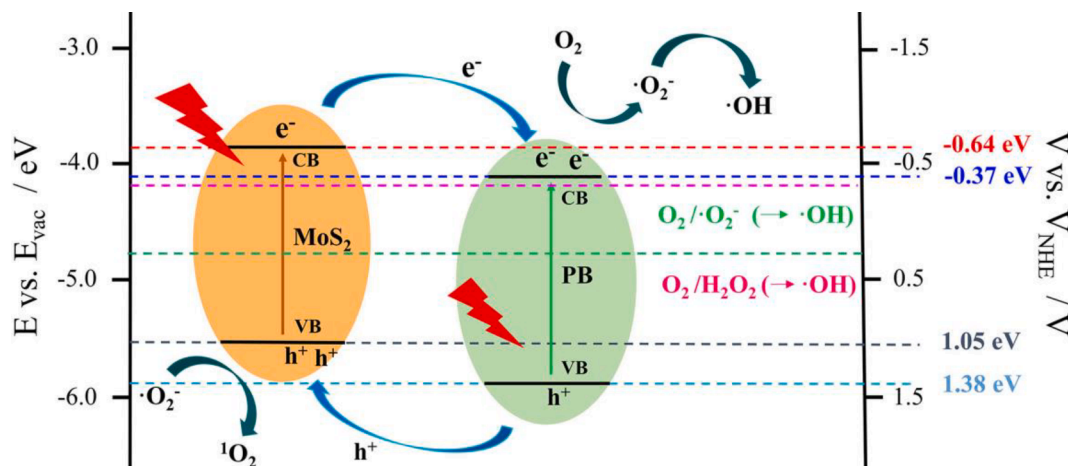


Fig. 5. Photocatalytic mechanism of ROS production after combining PB and MoS<sub>2</sub> under 660 nm irradiation.

two semiconductors in close contact, thus hindering the recombination of photogenerated charge. The details will be further discussed through the subsequent charge density difference and planar-averaged electron density difference.

Moreover, in addition to charge transfer at the heterointerface, the oxygen adsorption state on the material surface was also a significant factor for the generation of <sup>1</sup>O<sub>2</sub> and ·O<sub>2</sub><sup>-</sup>. The O<sub>2</sub> adsorption energy and the location of O<sub>2</sub> on different material surfaces (PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB) were further investigated by DFT calculations. In Fig. 4i, the O<sub>2</sub> adsorption site of MoS<sub>2</sub> was the S atom while for PB was the Fe (III) atom. For MoS<sub>2</sub>@PB, the O<sub>2</sub> binding site at the heterointerface were the S and Fe (III) atoms, respectively. As shown in Fig. 4j, the corresponding order of O<sub>2</sub> adsorption energy was MoS<sub>2</sub>@PB < PB < MoS<sub>2</sub>, thus demonstrating the optimal O<sub>2</sub> absorption capacity of the MoS<sub>2</sub>@PB heterostructure. Additionally, the 3D charge density difference of MoS<sub>2</sub>@PB is shown in Fig. 4k, in which the yellow and green areas represent charge accumulation and depletion, respectively. According to the planar-averaged electron density difference, there were approximately 0.000673 e/Å<sup>2</sup> electron transfers from PB to MoS<sub>2</sub> at the heterointerface by calculation (Fig. S11). The outcomes were consistent with Fig. 4g and 4 h. This demonstrated that an interfacial electric field was established between PB and MoS<sub>2</sub>, thereby promoting the separation of photoinduced carriers [57].

Besides the adsorption energy of oxygen, the oxygen activation energy is the most important parameter in the catalytic process of materials, and the foreign electrons transferred to the O<sub>2</sub> plays an important role in the oxygen activation [39]. Therefore, the Bader charge calculations and their charge density difference were performed via DFT calculations. Specifically, the direction and amount of charge transferred from MoS<sub>2</sub>, PB surfaces and MoS<sub>2</sub> heterojunction to O<sub>2</sub> molecule were shown in Fig. 4l, respectively. In the MoS<sub>2</sub> model, there was 0.124 electron charge from S atom to O<sub>2</sub> adatoms through the formed S—O bond, Whereas for PB model was 0.259 electron charge from Fe (III) atom to O<sub>2</sub> adatoms because of Fe—O (adatom) bonding. As for MoS<sub>2</sub>@PB, 1.663 and 1.654 electron charge were transferred from S and Fe (III) atoms to adsorbed O adatoms on account of the forming of S—O (adatom) bonding and Fe—O (adatom) bonding, respectively. The results of Bader charge calculations indicated that the MoS<sub>2</sub>@PB heterojunction can increase the amount of electron transfer to adsorbed O<sub>2</sub> molecules.

On the basis of the above experimental results, the mechanism of photocatalytic enhancement was given in Fig. 5. The band structure type of MoS<sub>2</sub>@PB is a typical type II heterostructure. When exposed to a 660 nm visible illumination, MoS<sub>2</sub> with a narrow bandgap of 1.69 eV could generate ROS. However, due to the severe electron-holes recombination and poor oxygen absorbing ability, a little amount of ROS was

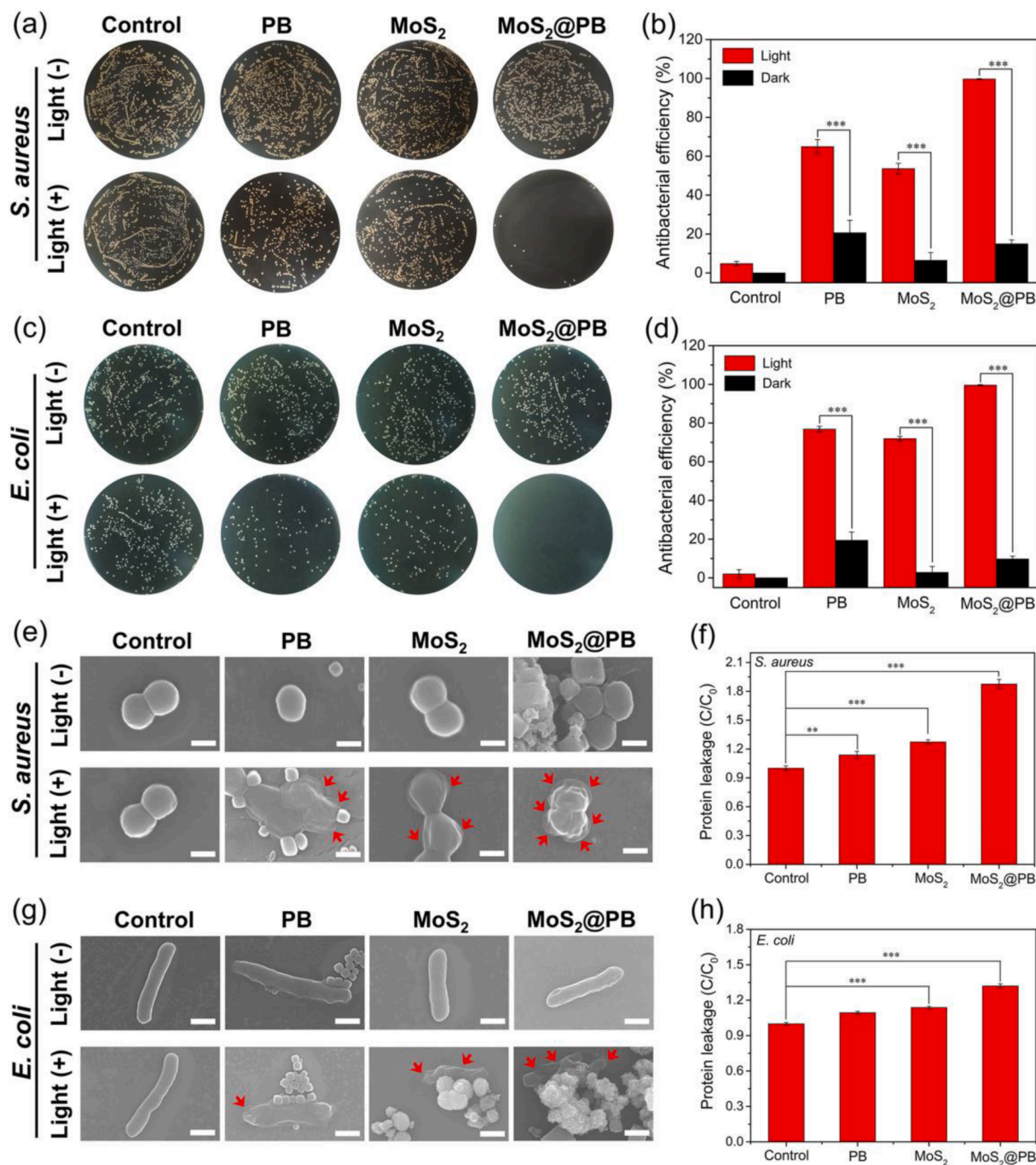
generated. When a core-shell heterogeneous interface was formed between the outer MoS<sub>2</sub> and the inner PB, the electron transport speed and separation efficiency of the photoinduced electrons and holes were accelerated, that was beneficial to the generation of ROS. The photocatalytic performance was also significantly improved.

As shown in Fig. 5, when irradiated by 660 nm light irradiation, MoS<sub>2</sub> and PB were excited to produce photoinduced charges in the CB and VB. Because MoS<sub>2</sub> has a more negative CB potential (-0.64 eV vs NHE) than PB (-0.37 eV vs NHE), photoexcited electrons on the MoS<sub>2</sub> surface could be transferred to PB, which facilitated the separation of photoexcited charges from MoS<sub>2</sub>. Additionally, since the CB potential of MoS<sub>2</sub> (-0.64 eV vs NHE) is more negative than the standard potential of O<sub>2</sub>/·O<sub>2</sub><sup>-</sup> (-0.33 eV vs NHE), the photoinduced electrons would react with O<sub>2</sub> molecules to generate ·O<sub>2</sub><sup>-</sup> [58], then the generated ·O<sub>2</sub><sup>-</sup> could further react with photoinduced holes to form <sup>1</sup>O<sub>2</sub>. Besides, ·OH was derived from the two-step translation route of ·O<sub>2</sub><sup>-</sup> in Fig. 5 [58,59]. Therefore, the above results confirmed that MoS<sub>2</sub>@PB composites had good photocatalytic activity with a 660 nm laser irradiation.

In Fig. 2a, since the incorporation of PB MOF significantly enhanced the light absorption intensity of MoS<sub>2</sub>@PB at 500–720 nm, MoS<sub>2</sub>@PB might possess an excellent photothermal performance under 660 nm illumination. Fig. S12a showed the heating curve of the samples with a 660 nm (power density: 0.4 W/cm<sup>2</sup>) laser irradiation. After 20 min of light, the temperatures of MoS<sub>2</sub> and PB increased from 26.8 °C to 53.5 °C and 64.5 °C, respectively. In contrast, the temperature of MoS<sub>2</sub>@PB increased from 26.8 °C to 57.8 °C under the same condition, suggesting that the combination with PB improved photothermal performance of MoS<sub>2</sub> under 660 nm light irradiation. The corresponding real-time infrared thermal images were shown in Fig. S12c. Beyond that, the repeatable rising/cooling curves shown in Fig. S12b further indicated that the photothermal property of the MoS<sub>2</sub>@PB was very stable after three irradiation cycles. The photothermal conversion efficiency (η) of MoS<sub>2</sub>@PB also was calculated shown in Fig. S13. Based on the corresponding maximum temperature and time constant (τ<sub>s</sub> = 224.54), the photothermal conversion efficiency of MoS<sub>2</sub>@PB was 39.30 %, which further demonstrated the high photostability of MoS<sub>2</sub>@PB under 660 nm red light illumination.

#### 3.4. Antibacterial study and the mechanism

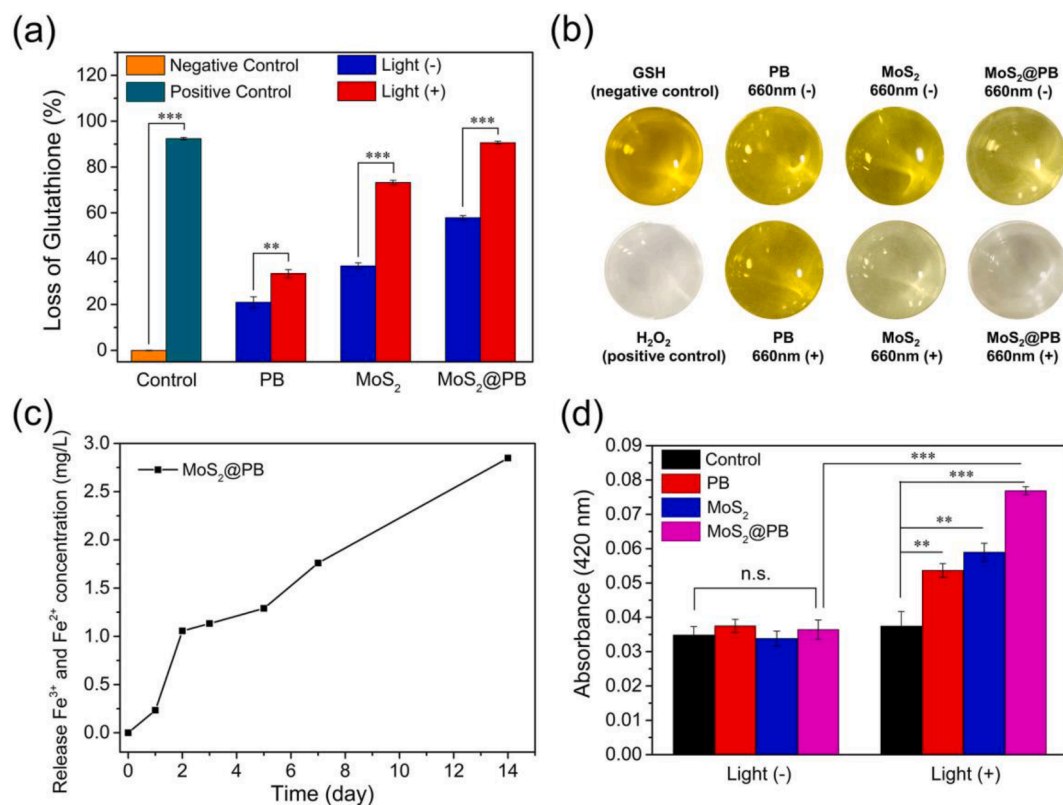
Two typical pathogens of *Staphylococcus aureus* (*S. aureus*, gram-positive) and *Escherichia coli* (*E. coli*, gram-negative), are commonly used as bacterial models in the bacterial-killing tests [60,61]. Here, they were utilized to study the antimicrobial property of various materials. The antibacterial properties of as-prepared materials *in vitro* were assessed using the spread plate method. As shown in Fig. 6a and 6c,



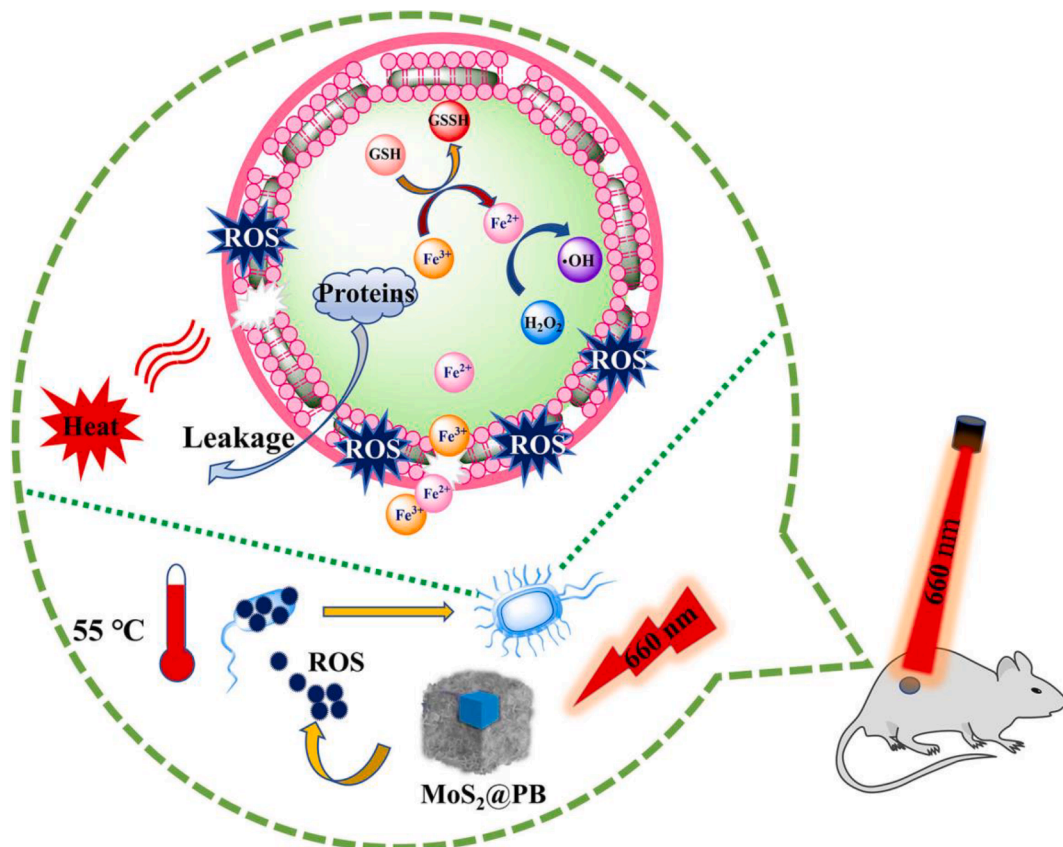
**Fig. 6.** The results of spread plate test of (a) *S. aureus* and (c) *E. coli* on different samples; The corresponding antimicrobial rates of the samples against (b) *S. aureus* and (d) *E. coli* according to the spread plate pictures; SEM photographs of the morphologies of (e) *S. aureus* (Scar bar = 500 nm) and (g) *E. coli* (Scar bar = 1  $\mu$ m) from different samples; Protein leakage of (f) *S. aureus* (h) *E. coli* after irradiation. (n = 3, mean  $\pm$  SD: \* $p$  < 0.05, \*\* $p$  < 0.01, \*\*\* $p$  < 0.001);

compared with the dark groups, the antibacterial efficacy of the corresponding light groups against *S. aureus* and *E. coli* were significantly enhanced. After 660 nm illumination for 20 min, the antibacterial efficiency of PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB were 64.97 %, 53.63 %, and 99.73 % against *S. aureus* (Fig. 6b) and 76.84 %, 71.93 %, and 99.58 % against *E. coli* (Fig. 6d), respectively. The antibacterial results suggested that the MoS<sub>2</sub>@PB group had the most excellent and fastest antibacterial activity under 660 nm light irradiation. Moreover, after three cycles of bacteria-killing tests, the MoS<sub>2</sub>@PB displayed circulatory antibacterial ratio over 99 % (Figs. S14b and S14d), and the corresponding spread plate images were shown in Figs. S14a and S14c. From these results, MoS<sub>2</sub>@PB exhibited good cycle sterilization performance and reusability. In order

to demonstrate the influence of hyperthermia and ROS on antibacterial performance. The antibacterial experiment was carried out by dividing into the following four groups: Control, MoS<sub>2</sub>@PB + Light (19  $^{\circ}$ C), MoS<sub>2</sub>@PB + Water-bath (55  $^{\circ}$ C), and MoS<sub>2</sub>@PB + Light (55  $^{\circ}$ C). The corresponding antibacterial efficiencies of MoS<sub>2</sub>@PB + Light (19  $^{\circ}$ C), MoS<sub>2</sub>@PB + Water-bath (55  $^{\circ}$ C), and MoS<sub>2</sub>@PB + Light (55  $^{\circ}$ C) were 36.84 %, 61.46 %, and 99.63 % shown in Fig. S15 respectively, which suggested hyperthermia alone has a higher bactericidal efficiency than ROS alone, and the antibacterial mode alone cannot achieve complete and effective killing of bacteria. In addition, the antibacterial properties of the materials under visible light irradiation were also evaluated as a comparison under 660 nm light irradiation. Fig. S16 exhibited that the

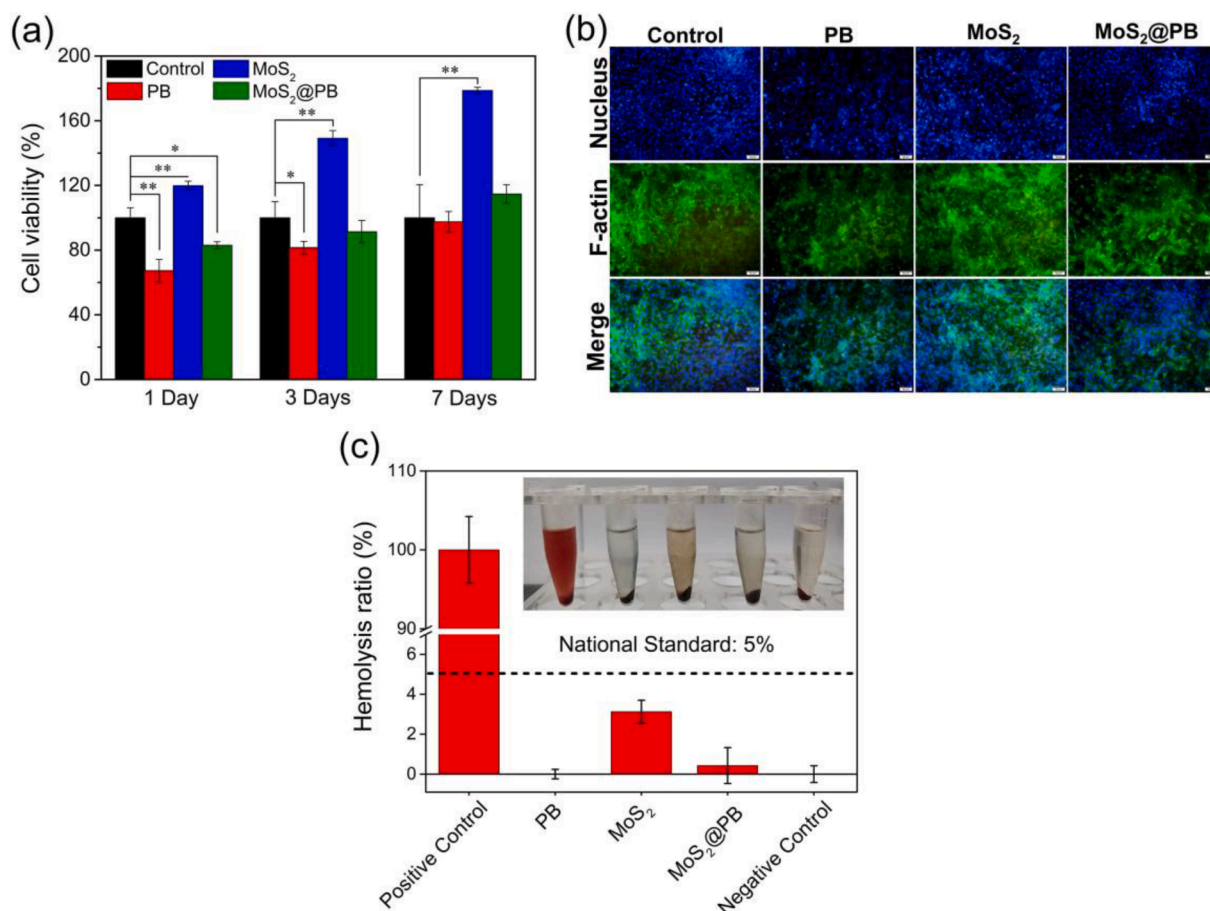


**Fig. 7.** (a) GSH deletion ability of PB, MoS<sub>2</sub> and MoS<sub>2</sub>@PB. (b) Corresponding discoloration photographs of different samples treated with GSH. (c) Cumulative amounts of Fe<sup>3+</sup> and Fe<sup>2+</sup> released from the MoS<sub>2</sub>@PB. (d) Membrane permeability of bacterial cells evaluated by ONPG hydrolysis assay on PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB. The error bars represent means  $\pm$  SD,  $n = 3$ . ns greater than 0.05, \* $p < 0.05$ , \*\* $p < 0.01$ , \*\*\* $p < 0.001$ .



**Fig. 8.** Bactericidal mechanism of optimized synergistic effect of hyperthermia, ROS and released ions for wound healing.





**Fig. 9.** (a) The viability of NIH-3 T3 cells cocultured with the materials at 1, 3, and 7 days. ( $n = 3$ ,  $*p < 0.05$ ,  $**p < 0.01$ ,  $***p < 0.001$ ). (b) Fluorescent staining images of cells after 1 day of incubation with different samples (scale bar = 50  $\mu\text{m}$ ). (c) Hemolysis rate of different samples.

antibacterial rates of PB, MoS<sub>2</sub> and, MoS<sub>2</sub>@PB under light were only 55.75 %, 59.18 %, and 74.02 % against *S. aureus* (Fig. S16b) and 59.08 %, 63.25 %, and 79.41 % against *E. coli* (Fig. S16d), respectively, indicating the lower bactericidal efficiency compared with 660 nm light irradiation.

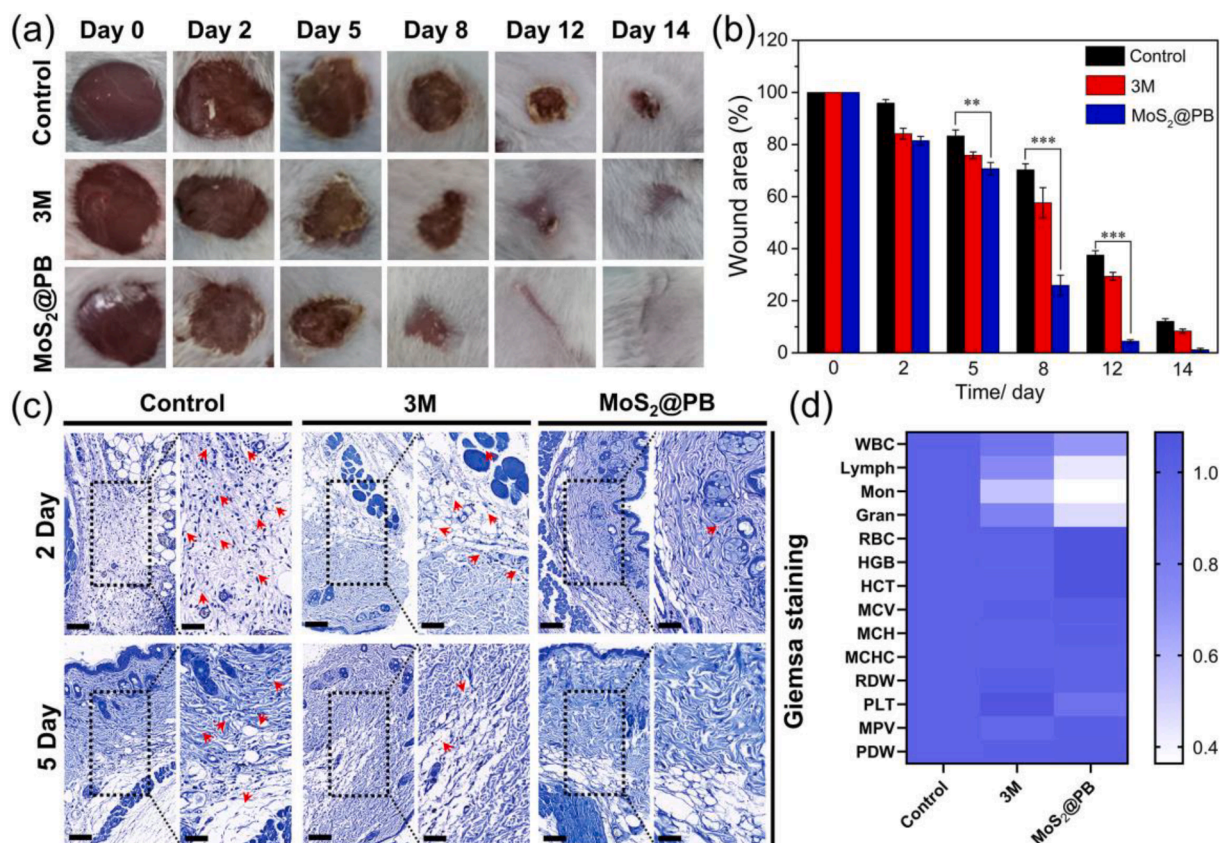
To further evaluate the antibacterial performance of materials, surface morphologies of different treated *S. aureus* and *E. coli* were observed by FE-SEM (Fig. 6e and 6 g). Under dark conditions, the bacteria of experimental groups or the control group maintained a smooth surface and intact shape, suggesting no obvious damage of bacterial membrane. By comparison, after 660 nm illumination for 20 min, the membranes of bacteria in the PB and MoS<sub>2</sub> groups were significantly wrinkled and damaged. Moreover, the bacterial membranes in the MoS<sub>2</sub>@PB group contracted more severely and even ruptured (signaled by red arrows), that attributed to the synergy effect of high temperature and abundant ROS generated by the MoS<sub>2</sub>@PB under illumination. Damage to cell membranes is often accompanied by severe protein leakage. As shown in Fig. 6f and 6 h, the MoS<sub>2</sub>@PB group with the highest antimicrobial efficiency under light had the most leaked proteins, which was also in line with the antibacterial results and bacterial morphology.

In order to intuitively observe the antibacterial activities, the viability of germs was qualitatively assessed by live/dead fluorescent staining assays, and the corresponding fluorescent images were shown in Fig. S17. The fluorescent images were mostly green under dark conditions, indicating that all materials showed negligible antibacterial properties in darkness. After 20 min of 660 nm laser illumination, partial red fluorescence clearly emerged in PB and MoS<sub>2</sub> groups, whereas almost no green fluorescence appeared in MoS<sub>2</sub>@PB group, indicating that MoS<sub>2</sub>@PB exhibited efficient antibacterial effect. These above

results were well in line with the spread plate results.

Glutathione (GSH), as a thiol-containing tripeptide, is the main endogenous antioxidant in bacteria and can be used as an important indicator of cellular oxidative stress. GSH can be converted to glutathione disulfide (GSSG) under oxidation conditions [43,44]. Ellman's assay was utilized to assess the GSH consumption capacity of materials. Fig. 7a showed the loss of GSH of different materials before and after illumination. After 20 min incubation with the materials in the dark, the loss of GSH in the PB and MoS<sub>2</sub> groups was 20.9 % and 36.8 % respectively. The weak oxidative ability of PB comes from the release of iron ions in PB, and MoS<sub>2</sub> also can facilitate oxidation of organic mercaptans (R-SH) to generate disulfide (R-S-S-R) [62]. As for MoS<sub>2</sub>@PB group, the consumption rate of GSH reached 57.8 % in the dark. When in light, the consumption percentage of GSH by PB increased slightly to 33.5 %. Comparatively, the loss of GSH of MoS<sub>2</sub> and MoS<sub>2</sub>@PB can reach up to 73.2 % and 90.6 %, respectively. The GSH loss caused by the MoS<sub>2</sub>@PB was higher than that by the MoS<sub>2</sub> under the same conditions. Apart from local hyperthermia and ROS yields, the rapid release of iron ions at high temperature can also induce reduction of GSH. The corresponding color change image after GSH processing was shown in Fig. 7b. The color of MoS<sub>2</sub>@PB faded almost completely under light, suggesting that GSH oxidation was the most severe, which corresponds well to the results shown in Fig. 7a. Furthermore, the existence of iron ions released from MoS<sub>2</sub>@PB was monitored by an inductively coupled plasma atomic emission spectrometry (ICP-AES) in Fig. 7c. The released Fe<sup>3+</sup> can oxidize the GSH in the bacteria and will be reduced to ferrous ions. The generated ferrous ions will further react with hydrogen peroxide in the bacteria to generate  $\cdot\text{OH}$  [35].

What is more, the bacterial membrane permeability was assessed by



**Fig. 10.** (a) In vivo antibacterial experiments and wound healing. (b) The process of wound healing ( $n = 3$ ,  $*p < 0.05$ ,  $**p < 0.01$ ,  $***p < 0.001$ ). (c) The Giemsa staining of wound tissue on days 2 and 5. The scale bars of the lower and higher magnification images are 50  $\mu\text{m}$  and 100  $\mu\text{m}$  respectively. (d) Blood routine parameters tested after 8 days of control, 3 M, and MoS<sub>2</sub>@PB groups treatment.

ONPG hydrolysis assay to further study the antibacterial mechanism [45,26]. Fig. 7d showed the OD<sub>420 nm</sub> value of the samples before and after illumination. The higher value of OD<sub>420 nm</sub> indicated the more serious membrane permeability. Under dark conditions, the PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB groups showed a negligible change at the OD<sub>420 nm</sub> value compared with the control group, suggesting unchanged bacterial membrane permeability. By contrast, the membrane permeability of the samples improved significantly under light conditions and the MoS<sub>2</sub>@PB group exhibited highest value of OD<sub>420 nm</sub>, which suggested that the synergy of moderate ROS and hyperthermia efficiently increased the membrane permeation of bacteria, thereby the iron ions can more easily penetrate bacterial membrane [63,37]. These results indicated that MoS<sub>2</sub>@PB could rapidly kill bacteria under light irradiation due to local hyperthermia, abundant ROS and the released iron ions.

Herein, a possible bacteria-killing mechanism was schematically illustrated in Fig. 8. When the MoS<sub>2</sub>@PB irradiated with 660 nm laser irradiation, bacteria in the surrounding the environment were attacked by ROS generated from MoS<sub>2</sub>@PB, causing initial oxidative lesions to the bacterial membranes and making the bacteria to be more sensitive to heat [64]. Meanwhile, the elevated temperature produced by the MoS<sub>2</sub>@PB under light increased the permeability of bacterial membrane, thus making it easier for iron ions to penetrate the bacterial cell wall and realize the Fenton reaction [35]. Subsequently, the disturbed bacteria continued to be damaged, resulting in bacterial membrane brake and protein leakage. In addition, the MoS<sub>2</sub>@PB produced the hyperthermia, more ROS, and prereduced small amount iron ions, which could accelerate the oxidation of GSH to GSSG. Consequently, the intrinsic balance of the bacteria's protective environment was destroyed, which eventually led to bacterial death. In summary, the synergistic action of hyperthermia and ROS make MoS<sub>2</sub>@PB

nanocomposites possess excellent antibacterial performance.

### 3.5. In vitro biocompatibility evaluation

The cytocompatibility of samples was studied by a 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT) method. In Fig. 9a, after 1 day' culture, the MoS<sub>2</sub> group exhibited higher cell viability (119.87 %) than PB (67.34 %) and MoS<sub>2</sub>@PB (83.02 %) groups compared with the control group, which attributed to the excellent biocompatibility of MoS<sub>2</sub>. This is because the lamellar structure of MoS<sub>2</sub> with a rough surface is beneficial for cellular adhesion and growth [65]. The PB group exhibited slight cytotoxicity due to the excess of released iron ions. However, after 3 and 7 days of culture, with the increase of cultivation time, the cell viability of PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB was over 80 % and 90 %, respectively. The above results indicated the great cytocompatibility of PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB. Also, the cell fluorescent staining was conducted to further investigate cytotoxicity of the samples (Fig. 9b). After 1 day' culture, compared with the PB group, the NIH-3 T3 cells in MoS<sub>2</sub> and MoS<sub>2</sub>@PB groups showed more filopodia extensions around, suggesting that the introduction of MoS<sub>2</sub> facilitated fibroblasts to migration and proliferation. It has been reported that this may possibly be due to the high specific surface area of the nanosheet structure of MoS<sub>2</sub>, which can promote cell growth and anchoring of filopodia [66,67,32]. Besides that, the cell density of MoS<sub>2</sub>@PB increased significantly because of the good biocompatibility of MoS<sub>2</sub>. This outcome was in accordance with MTT assay and could further demonstrate that MoS<sub>2</sub>@PB had the great cytocompatibility.

In addition, hemolysis tests were used to evaluate the hemolytic activity of materials. Fig. 9c showed that the hemolysis rate of PB, MoS<sub>2</sub>, and MoS<sub>2</sub>@PB were below internationally recognized standard (5 %), indicating good blood compatibility of materials [68].



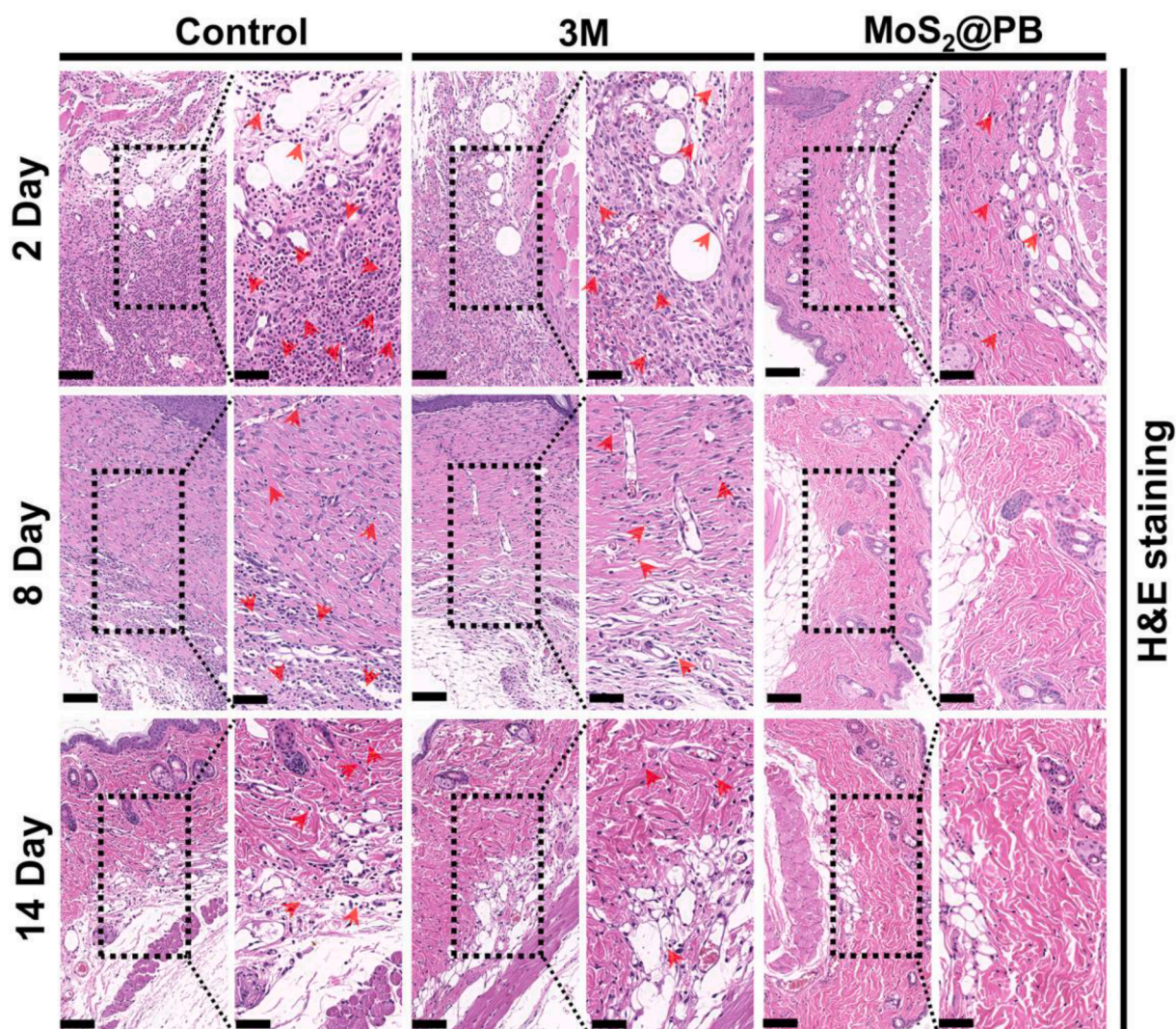


Fig. 11. The H&E staining of wound tissue in all groups on days 2, 8, and 14. Scale bars: 50  $\mu\text{m}$  (high resolution) and 100  $\mu\text{m}$  (low resolution).

### 3.6. *In vivo* antibacterial test and wound healing

Animal models were conducted to assess the antimicrobial effect of the samples in wound infection and the effect on wound healing. Fig. 10a evaluated the wound healing process of different samples (control group, 3 M group, MoS<sub>2</sub>@PB group). The control and 3 M dressing groups exhibited severe bacterial infection after day 2 of treatment, while the experimental group had fewer bacterial infections, which was in accordance with the *in vitro* antibacterial activity (Fig. 6). After 5, 8, 12, and 14 days of treatment, in comparison with the control and the 3 M groups, the experimental group had the best wound healing rate, and the wound healed completely after 14 days. To clearly observe the speed of wound healing, the quantified changes in wound area over time were shown in Fig. 10b, confirming that the wounds treated with MoS<sub>2</sub>@PB healed the fastest. The experimental results showed that MoS<sub>2</sub>@PB expressed certain antibacterial and anti-inflammatory effects during the treatment process.

To further investigate wound inflammation, Giemsa and H&E staining were used to examine the recovery of differently treated wounds [63]. The amount of bacteria adhering to the wound on days 2 and 5 was observed by Giemsa staining in Fig. 10c. After 2 days, a large number of bacteria appeared in the control and 3 M groups (indicated by red arrows), while the number of bacteria appeared in MoS<sub>2</sub>@PB was less. After 5 days, there were still obvious bacterial residues in the

control group. On the contrary, the bacterial number in the MoS<sub>2</sub>@PB group was significantly reduced. This suggested that the synergistic antibacterial effect achieves a rapid sterilization and hinders bacterial infection in the body. In addition, Fig. 11 showed histological images of H&E staining after 2, 8, and 14 days. After 14 days, inflammatory cells were still present in the control and 3 M groups, while the MoS<sub>2</sub>@PB group had almost no inflammatory cells and most cells were normal. The above experimental results indicated that MoS<sub>2</sub>@PB has good antibacterial properties and wound healing ability.

In addition, whole blood of mice in all treatment groups was collected on day 8 for routine blood analysis. As shown in Fig. 10d, the number of white blood cells, lymphocytes, and neutrophils in the control and 3 M groups in the blood routine were obviously higher than that in the material group, suggesting that the MoS<sub>2</sub>@PB group had the least amounts of inflammatory cells and the least inflammation in the mice. Furthermore, the hemoglobin concentration (HGB), the number of red blood cells (RBC) and the hematocrit (HCT) in the MoS<sub>2</sub>@PB group were remarkably greater than that of the control and 3 M groups. This is because the hemoglobin molecular formula consists of four molecules of hemoglobin and four molecules of heme, and the slow release of Fe<sup>2+</sup> contributes to the production of hemoglobin. Besides, there were no significant differences in blood routine parameters between the different groups. Routine blood data again demonstrated that MoS<sub>2</sub>@PB possessed the best therapeutic effect on bacterial infection *in vivo*.



As shown in Fig. S18, after 14 days of treatment, the H&E staining of the main organs (heart, liver, spleen, lung and kidney) of mice in different groups did not exhibit any abnormal damage, indicating that MoS<sub>2</sub>@PB had no obvious damage to the treated tissue and can be employed for long-term treatment of wounds.

#### 4. Conclusion

In summary, bio-functionalized MoS<sub>2</sub>@PB composite was successfully prepared and first explored for rapid sterilization. The photodynamic mechanism at the heterointerface was verified by theoretical calculations based on energy evolution pathways and charge transfer. In addition to the rapid transport of photogenerated charges and the suppresses of photocarriers recombination between PB and MoS<sub>2</sub>, the photocatalytic activity of MoS<sub>2</sub>@PB were significantly enhanced due to the lower O<sub>2</sub> adsorption energy and higher charge transfer amount toward the adsorptive O<sub>2</sub>. Furthermore, the photothermal effect of the system was improved due to the introduction of PB. The MoS<sub>2</sub>@PB had good chemical stability and repeated photothermal stability. When exposed to 660 nm visible light irradiation, MoS<sub>2</sub>@PB exhibited an antimicrobial efficiency of 99.73 % and 99.58 % against *S. aureus* and *E. coli* severally within 20 min. Also, the oxidation of GSH to GSSG was accelerated through the synergy action of generated ROS, hyperthermia, and the released iron ions. Owing to the low toxicity of the material, the MoS<sub>2</sub>@PB had good biocompatibility. Synchronously, from the treatment results of the wound infection model, MoS<sub>2</sub>@PB can quickly kill bacteria in the wound and inhibit inflammation to promote wound healing. The blood routine results also showed that the experimental group had a higher hemoglobin level than other groups because of the slow release of iron ions. We believe that this study will bring new perspectives for the development of safe, rapid, controllable, and highly effective therapeutic strategies.

#### 5. Data availability

Data will be made available on request.

#### Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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#### Appendix A. Supplementary data

Supplementary data to this article can be found online at <https://doi.org/10.1016/j.cej.2022.139127>.

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